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- Published: July 31, 2013
- <http://dx.doi.org/10.1371/journal.pone.0069812>

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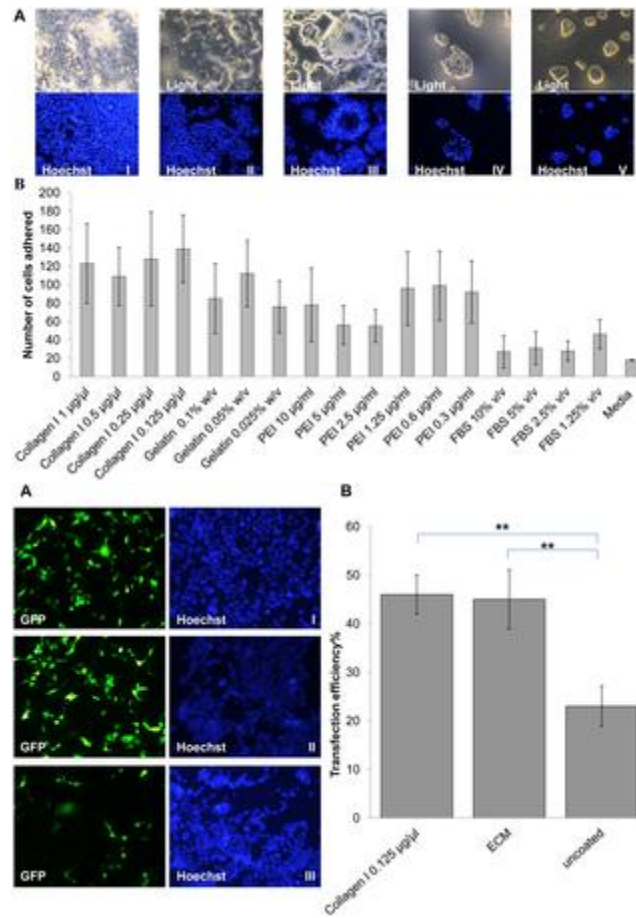
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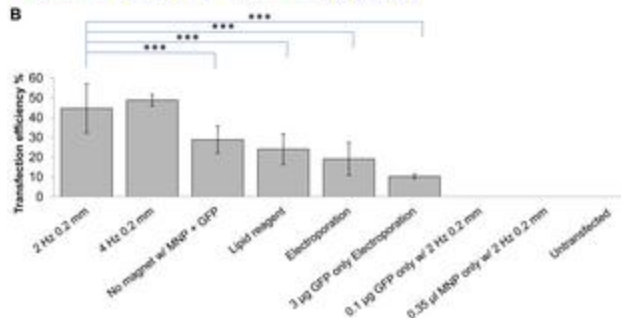
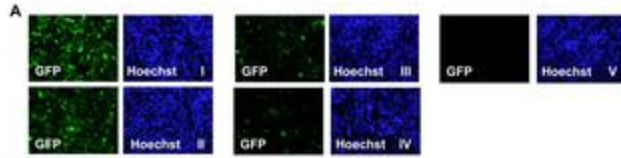
## Abstract

Magnetic nanoparticle-based gene transfection has been shown to be an effective, non-viral technique for delivery of both plasmid DNA and siRNA into cells in culture. It has several advantages over other non-viral delivery techniques, such as short transfection times and high

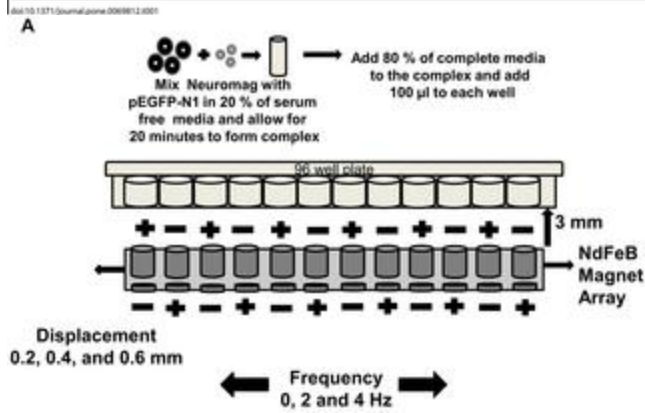
cell viability. These advantages have been demonstrated in a number of primary cells and cell lines. Here we report that oscillating magnet array-based nanomagnetic transfection significantly improves transfection efficiency in both human prenatal cardiac progenitor cells and adult cardiomyocytes when compared to static magnetofection, cationic lipid reagents and electroporation, while maintaining high cell viability. In addition, transfection of adult cardiomyocytes was improved further by seeding the cells onto Collagen I-coated plates, with transfection efficiencies of up to 49% compared to 24% with lipid reagents and 19% with electroporation. These results demonstrate that oscillating nanomagnetic transfection far outperforms other non-viral transfection techniques in these important cells.

## Figures

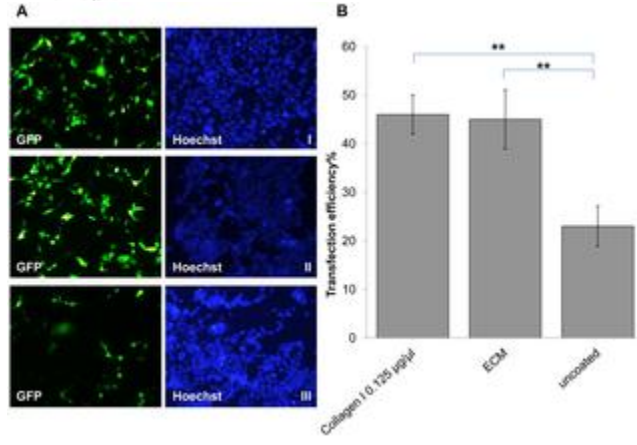
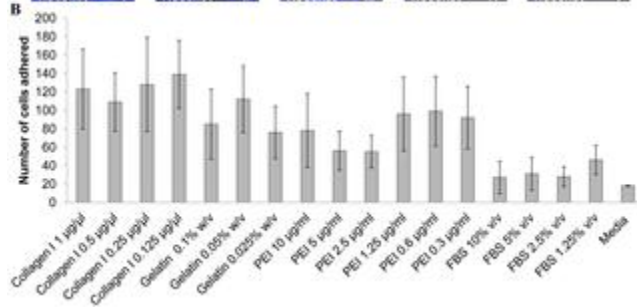
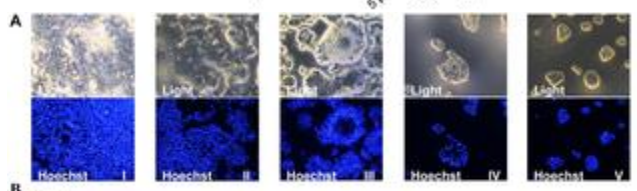
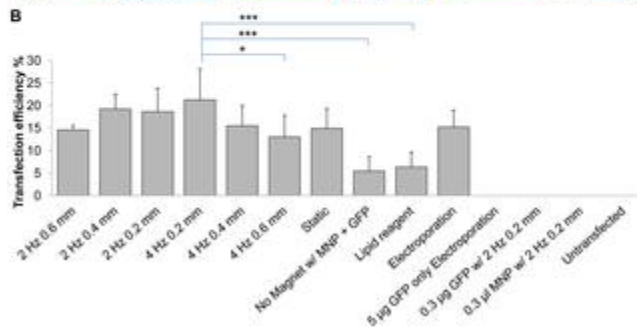
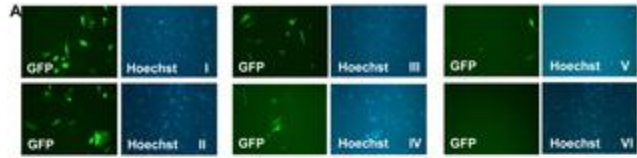


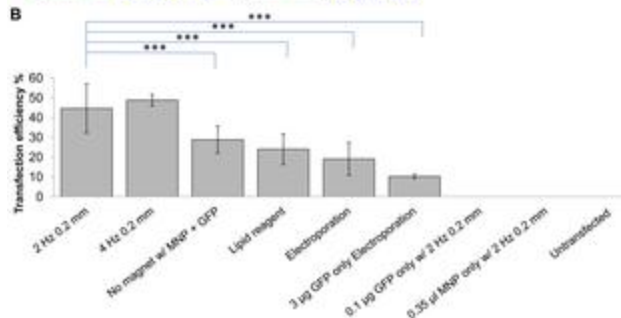
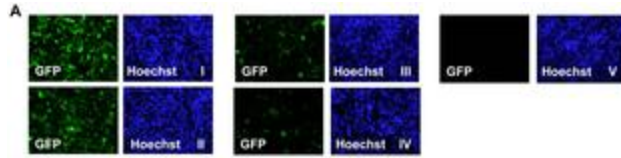


Cell type	Source	Transfection method	Transfection efficiency
Cardiovascular system cells	Chicken	Adenoviral vector	63% [38]
Cardiomyocytes	Rat	Adenoviral vector	90% [39]
Cardiomyocytes	Rat	Adenoviral vector	100% [40]
Cardiomyocytes	Rat	Adeno associated viral vector	90% [40]
Cardiomyocytes	Rat	Adeno associated viral vector	88.1% [41]
Cardiomyocytes	Rat	Adenoviral-polylysine vector	70% [42]
Cardiomyocytes	Rat	Retroviral/Lentiviral vector	70-100% [40]
Cardiomyocytes	Rat	Calcium phosphate precipitate	1-2% [43]
Cardiomyocytes	Rat	Calcium phosphate precipitate	5-8% [47]
Cardiomyocytes	Rat	Calcium phosphate precipitation method	2-4% [43]
Cardiomyocytes	Rat	Calcium phosphate precipitation method	5-10% [34]
Cardiovascular system cells	Chicken	Electroporation	26% [38]
Cardiomyocytes	Rat	Electroporation	7.5% [41]
Cardiomyocytes	Rat	Electroporation	37% [40]
Cardiomyocytes	Rat	Nucleofection	4.8% [41]
Cardiomyocytes	Rat	Nucleofection	70% [40]
Cardiomyocytes	Rat	Lipofectin	1.6% [42]
Cardiomyocytes	Rat	Lipofectamine 2000	8.1% [41]
Cardiomyocytes	Rat	Fugene 6	3.3% [41]
Cardiomyocytes	Rat	Optical transfection	5% [45]
Cardiovascular system cells	Hamster	Hypothermic cardioplegia method	77.3±9.2% [46]
Cardiomyocytes	Rat	Pressure mediated transfection	48.1±1% [45]
Cardiomyocytes	Pig	Adenoviral vector	[46]
Cardiomyocytes	Rat	Adeno associated viral vector	[47]
Cardiac progenitor cells	Mouse	Bioelectric lentiviral vector	[48]
Cardiovascular system cells	Dog	Hemagglutinating virus of Japan-liposome method	[49]
Cardiovascular system cells	Rat	Hemagglutinating virus of Japan-liposome method	[50]
Cardiomyocytes	Rat	Liposomes coated with or inactivated sendai viral vector	[47]
Cardiomyocytes	Rat	Lipofectamine plus	[47]
Cardiomyocytes	Rat	Geneporter	[47]
Cardiomyocytes	Rat	Maxfectene	[47]
Cardiomyocytes	Rat	Lipogen	[47]
Cardiovascular system cells	Rat	Ultrasound-targeted liposome microbubble destruction	[51]
Cardiovascular system cells	Dog	DNA-polymer coating	[52]
Cardiac progenitor cells	Human	The pNC1 integrase genomic modification system	[53]

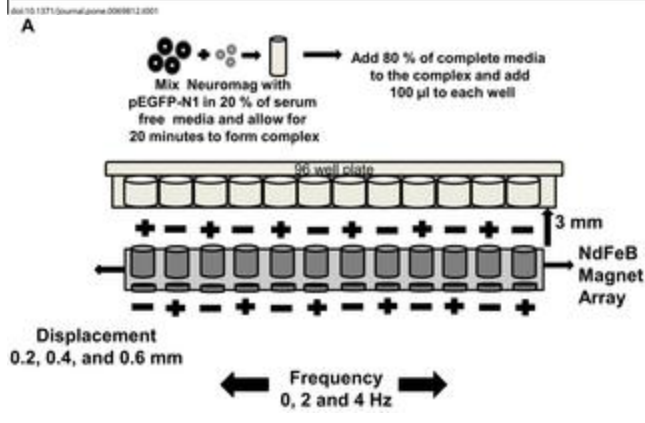


doi:10.1371/journal.pone.0089812.g001

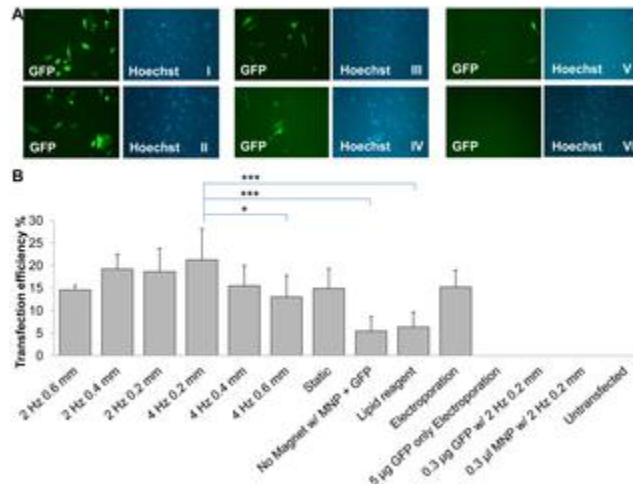




Cell type	Source	Transfection method	Transfection efficiency
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Cardiac progenitor cells	Human	The pNCT integrase genomic modification system	[53]



doi:10.1371/journal.pone.0089812.g001



**Citation:** Subramanian M, Lim J, Dobson J (2013) Enhanced Nanomagnetic Gene Transfection of Human Prenatal Cardiac Progenitor Cells and Adult Cardiomyocytes. PLoS ONE 8(7): e69812. doi:10.1371/journal.pone.0069812

**Editor:** Bing Xu, Brandeis University, United States of America

**Received:** February 12, 2013; **Accepted:** June 12, 2013; **Published:** July 31, 2013

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**Funding:** This research was funded by nanoTherics limited. The funders had no role in study design, data collection and analysis, decision to publish, or preparation of the manuscript.

**Competing interests:** Commercialisation of the oscillating nanomagnetic gene transfection technique on the magnetfect system was carried out by nanoTherics Limited.

## Introduction

The discovery, isolation and differentiation of human cardiac progenitor cells from the epicardium of the heart has given scientists and clinicians alike a tangible opportunity to investigate cardiovascular diseases as well as other issues concerning tissue regeneration [1], [2], [3], [4]. Cardiac progenitor cells, with their ability to differentiate into cardiomyocytes, fibroblasts and coronary vessels *in vitro*, are unique in their ability to replace damaged cardiac tissue in cardiovascular cell therapy [5], [6]. The isolation of primary adult human cardiomyocytes has made it possible to formulate *in vitro* models to understand the human heart and cardiac diseases [7], identify the different cardiomyocytes present [8], and study cardiomyocyte differentiation to address tissue regeneration [9]. However, despite these advances, successes in cardiovascular gene therapy still remains elusive and non-viral transfection of cardiomyocytes suffers from poor efficiency and relatively low cell viability.

There are more than 3,000 genetic disorders that arise as a result of single gene alterations. In the cardiovascular system disorders such as atrioventricular conduction delay, atrial septal defects, early valve calcification and endocardial cushion effect, all involve single gene alterations [10]. Understanding these mutations and their resulting disorders remains crucial in our search for a cure. While it may be possible to identify a disease-causing gene, delivery of genetic material

into a cell to correct the defective gene remains a challenge. Currently, this is achieved mostly by using non-infective viruses, cationic lipid reagents and electroporation *in vitro* (Table 1). Most gene delivery approaches are not been widely applicable due to low transfection efficiency or the lack of suitable vectors, target specificity, or safety issues arising from translating the technique into humans [11].

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Cardiomyocytes	Rat	Nucleofection	4.8% [41]
Cardiomyocytes	Rat	Nucleofection	70% [40]
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**Table 1. Review of methods used for transfecting cardiovascular system cells.**

<http://dx.doi.org/10.1371/journal.pone.0069812.t001>

In order to overcome these problems there is a critical need for an efficient, biocompatible and remotely controllable method of transfection. The use of magnetic nanoparticles (MNPs) has numerous applications in the field of biomedicine such as targeted drug delivery; diagnostics combined with therapeutics (i.e. magnetic resonance-guided stem cells labelled with MNPs for cell replacement therapy); MNP labelled-cell sorting; localised hyperthermia for the treatment of solid tumours, remote control of cell processes, and external magnetic field mediated gene delivery [12], [13], [14], [15].

Nanomagnetic transfection is a non-viral gene delivery technique that uses magnetic force acting on superparamagnetic nanoparticles (SPIONs) onto which plasmid DNA or siRNA is adsorbed. High gradient, rare earth magnets placed below the culture plate direct the MNP/DNA complexes into contact with cells and oscillating the magnet array induces endocytosis of the complex, after which the DNA is released into the cytoplasm [16], [17]. The advantages of magnetofection *in vitro* are: 1) low amounts of transfection complexes; 2) high cell viability; 3) high transfection efficiency; 4) little or no interference with cell proliferation and differentiation [18], [19], [20], [21], [22], [23], [24]. Although biocompatible MNPs have been



developed specifically for magnetofection in various cell types with a stationary magnet array[19], [23], there have been no reports of the use of an oscillating magnet array during transfection of human prenatal cardiac progenitor cells and adult cardiomyocytes. Here we demonstrate the *in vitro* delivery of the reporter plasmid pEGFP-N1 using the oscillating magnet array and MNPs in human prenatal cardiac progenitor cells and adult cardiomyocytes and compare it to other non-viral transfection techniques.

## Materials and Methods

### Cells and Reagents

Human prenatal cardiac progenitor cells (Cambridge Bioscience, Cambridge, UK) and adult cardiomyocytes (Celprogen, California, USA) were purchased, cultured and maintained in standard tissue culture flasks containing horse serum supplemented Cardiac Cellutions medium (Cambridge Bioscience, Cambridge, UK) or in Extra Cellular Matrix (ECM) coated tissue culture flasks (Celprogen, California, USA) containing human cardiomyocytes cell culture complete media with serum and antibiotics (Celprogen, California, USA). The pEGFP-N1 (Clontech, California, USA), a 4.7 kb plasmid containing a CMV promoter and gene expressing enhanced Green Fluorescent Protein (eGFP) was used as a reporter for this study. The plasmid DNA was purified using EndoFree Plasmid Purification kit (Qiagen, Crawley, UK) and maintained at  $-80^{\circ}\text{C}$  in endonuclease-free water (Sigma, Dorset, UK).

### Adhesion Assay

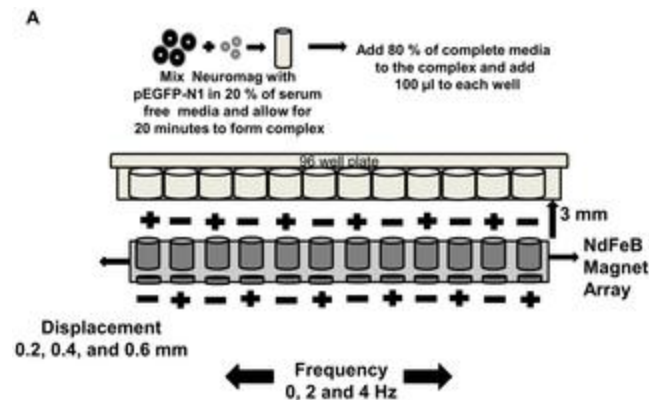
As human adult cardiomyocytes are a semi-adherent cell type, adhesion studies were performed. 96 well tissue culture plates (Corning, New York, USA) were coated with foetal bovine serum (FBS: 10, 5, 2.5, and 1.25%) (Lonza, Cologne, Germany), polyethyleneimine (PEI: 10, 5, 2.5, 1.25, 0.6 and 0.3  $\mu\text{g}/\text{ml}$ ) (Sigma, Dorset, UK), gelatin (0.1, 0.05 and 0.025% w/v) (Sigma, Dorset, UK) and rat tail collagen I (1, 0.5, 0.25 and 0.125  $\mu\text{g}/\text{ml}$ ) (Sigma, Dorset, UK), made up in phosphate buffer saline (PBS) and incubated overnight at  $4^{\circ}\text{C}$ . Following incubation the coated plates were washed once with PBS, 20,000 human adult cardiomyocytes were seeded onto coated wells and incubated overnight at  $37^{\circ}\text{C}$  with 5%  $\text{CO}_2$ . 24 h post seeding, the wells were washed twice with PBS and stained with 2 mg/ml nuclear Hoechst-33342 stain (Sigma, Dorset, UK) at 1  $\mu\text{l}$  per well. Cells adhered per field were imaged and phenotypes were recorded.

### Nanomagnetic Transfection

10,000 progenitor cells and 20,000 cardiomyocytes per well were seeded into 96 well tissue culture plates previously coated with 0.8  $\mu\text{g}/\mu\text{l}$  rat tail collagen I, and onto extra cellular matrix coated tissue culture treated 96 well plates (Celprogen, California, USA) in 100  $\mu\text{l}$  complete growth media and incubated for 24 h at  $37^{\circ}\text{C}$  with 5%  $\text{CO}_2$ . Prior to transfection, 0.05 or 0.1  $\mu\text{g}$  of pEGFP-N1 formed complexes with 0.2 or 0.35  $\mu\text{l}$  NeuroMag (nanoTherics, Keele, UK) for 15 minutes in serum-free growth media containing antibiotics (Celprogen, California, USA) ([Figure 1](#)). NeuroMag, a MNP transfection vector was used for its non-interference with proliferation and low cytotoxicity, as observed during transfection of oligodendrocyte progenitor cells [19] and



neural precursor/stem cells [21], [23]. After complex formation, 80  $\mu$ l of complete medium was added, mixed and transferred, drop-wise, onto the appropriate well(s) containing prenatal human cardiac progenitor cells or adult cardiomyocytes. Plates were placed on a 96 well oscillating NdFeB (Rare earth magnet, an alloy of neodymium, iron and boron) magnet array following the magnefect nano II system protocol (Figure 1). Following 30 minutes exposure to the oscillating magnetic array, the culture plate was removed from the system and incubated at 37°C with 5% CO<sub>2</sub> for 48 h. Lipofectamine 2000 (Invitrogen, Paisley, UK) and Nucleofector 2b (Lonza, Cologne, Germany) were evaluated for comparison and transfections were performed according to the manufacturer's instructions.



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**Figure 1. Oscillating nano-magnetofection 96 well experimental setup (a) Diagrammatic representation of a 96 well oscillating magnet array-based nanomagnetic transfection setup using NdFeB magnetic array.**

<http://dx.doi.org/10.1371/journal.pone.0069812.g001>

## Cell Viability Assay

CytoTox-ONE™ homogenous membrane integrity assay (Promega, Southampton, UK) provided the measure of released lactate dehydrogenase (LDH) through damaged membrane of dead cells and the assay was performed according to manufacturer's instruction. Fluorescence was recorded at excitation wavelength 560 nm and emission wavelength 590 nm using a fluorescent plate reader (BioTek, Bedfordshire, UK). Viability data is expressed as a percentage using the following formula.

Percentage viability =  $100 - [100 \times (\text{Experimental} - \text{Background fluorescence}) / (\text{Maximum LDH release} - \text{Background fluorescence})]$ .

## Microscopy Analysis

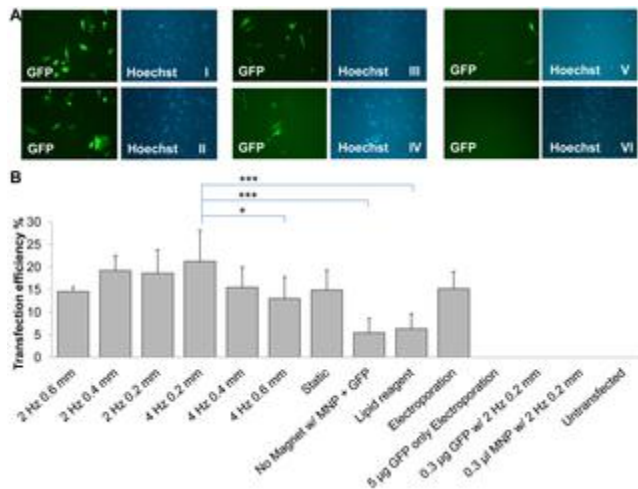
48 h post transfection, cells were stained with 2 mg/ml Hoechst-33342 (nuclear) stain at 1  $\mu$ l per well to ensure that only viable cells were counted while correlating GFP expressing cells. Both

GFP expression and Hoechst fluorescence was observed using an epifluorescent microscope (Olympus IX51, Essex, UK). A semi-quantitative analysis of transfection efficiency was determined by counting the number of GFP-expressing cells versus the total number of Hoechst stained cells using the cell counting feature of ImageJ software (National Institute of Health, USA). Cell viability was determined by counting the number of cellTrace™ calcein red-orange-AM (Invitrogen, Paisley, UK) versus the total number of Hoechst stained cells and phase contrast microscopic image of cells using ImageJ software. Statistical significance was calculated using one-way analysis ANOVA with Bonferroni's multiple comparison test (GraphPad Prism v6.01, California, USA).

## Results

### Oscillating Magnet Array-based Nanomagnetic Transfection of Human Cardiac Progenitor Cells

In prenatal human cardiac progenitor cells approximately 18.6±5.2% transfection efficiency was observed when the complexes were subjected to an NdFeB magnet array oscillating at a frequency of 2 Hz with a displacement of 0.2 mm (Figure 2). Different oscillating frequencies (0, 2 and 4 Hz) and displacements (0.2, 0.4, 0.6 mm) were evaluated in order to ascertain their impact. Initial results were improved to 21.3±6.8% transfection efficiency using a magnet array oscillating at 4 Hz, with a 0.2 mm displacement. This appeared to be the optimum frequency/amplitude combination in this case and there was a decrease in transfection efficiency when compared to 2 Hz/0.2 mm (18.6±5.2%), 2 Hz/0.4 mm (19.2±3.3%,  $p>0.05$ ) and 2 Hz/0.6 mm (14.6±0.9%,  $p>0.05$ ), 4 Hz/0.4 mm (15.5±4.5%), and 4 Hz/0.6 mm (13.0±4.8%,  $*p<0.05$ ). The 4 Hz/0.2 mm group also outperformed the no magnet control (5.5±3.2%,  $**p<0.001$ ), static magnetofection (14.9±4.4%), cationic lipid-based transfection (6.3±3.4%,  $***p<0.001$ ), and electroporation (15.2±3.8%) (Figure 2). While there appears to be a suggestion of some systematic variation in transfection efficiency with displacement at 4 Hz, the relationship is not statistically significant across all three displacements and is not seen in the 2 Hz groups.



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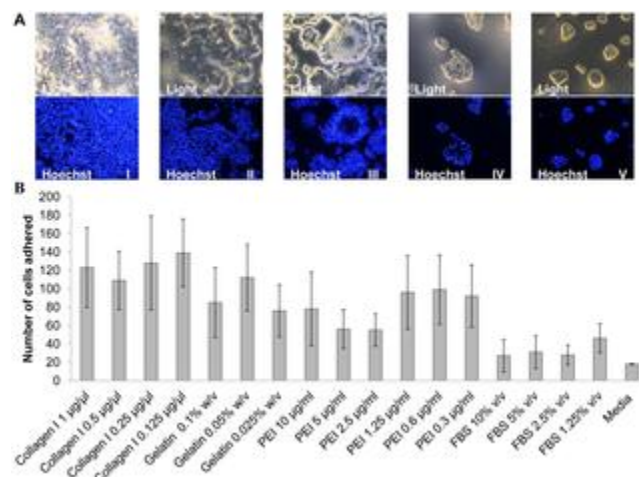
### Figure 2. Comparison of prenatal human cardiac progenitor cells transfected using oscillating magnet array-based nanomagnetic transfection.

(a) Fluorescent microscope images of prenatal human cardiac progenitor cells transfected with pEGFP-N1 representing each conditions, took 48 h post transfection. (I) GFP fluorescence and Hoechst image for 2 Hz 0.2 mm, (II) GFP fluorescence and Hoechst image for 4 Hz 0.2 mm, (III) GFP fluorescence and Hoechst image for static magnetofection™, (IV) GFP fluorescence and Hoechst image for electroporation (V) GFP fluorescence and Hoechst image for lipid based transfection reagent, (VI) GFP fluorescence and Hoechst image for un-transfected (b) Prenatal human cardiac progenitor cells were transfected with pEGFP-N1 as indicated, and scored using manual counting using ImageJ software, 48 h after transfection. Data shown are the media ± SD. n=12 for 4 Hz 0.2 mm. n=9 for 2 Hz 0.2 mm and static conditions. n=6 for 4 Hz 0.4 mm, 4 Hz 0.6 mm, no magnet, electroporation and pEGFP-N1 only electroporation conditions. n=3 for 2 Hz 0.4 mm, 2 Hz 0.6 mm, pEGFP-N1 only, Neuromag only, and un-transfected conditions. (\*p<0.05, \*\*\*p<0.001 - Statistically significant).

<http://dx.doi.org/10.1371/journal.pone.0069812.g002>

## Cell Adhesion Assay

In the adhesion studies, cells adhered better to wells coated with rat tail collagen I (0.125, 0.25, 0.5, 1 µg/ml), when compared to gelatin from bovine serum (0.05, 0.1, 0.025% W/v), polyethyleneimine (0.6, 1.25, 0.3, 10, 5, 2.5 µg/ml) and foetal bovine serum (1.25, 5, 2.5, 10% v/v). Morphologically, cells seeded onto collagen I, gelatin-, FBS- and un- coated wells were normal in appearance, unlike cells seeded in polyethyleneimine-coated wells, which, though adhering, they were rounded, gathered in clusters with compacted nucleus and a high levels of cell debris were observed. With the latter case, cells were also observed to detach from the surface after washing (Figure 3). Cardiomyocytes being a semi-adherent cell type, collagen I was found to be a suitable coating to enhance adhesion in cardiomyocytes to aid adherent state transfection.



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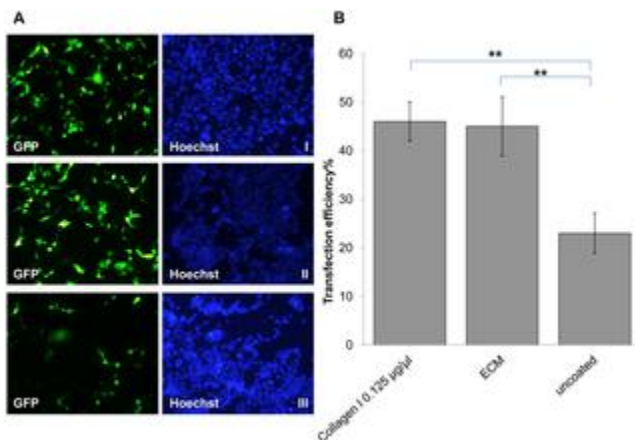
### Figure 3. Adhesion studies in adult human cardiomyocytes.

(a) Light and Fluorescent microscope images of adult human cardiomyocytes seeded onto different coatings, took after overnight incubation. (I) Light and Hoechst image for collagen 1 coating (0.125  $\mu\text{g}/\mu\text{l}$ ), (II) Light and Hoechst image for gelatine coating (0.05% w/v), (III) Light and Hoechst image for polyethyleneimine coating (0.6  $\mu\text{g}/\text{ml}$ ), (IV) Light and Hoechst image for foetal bovine serum coating (1.25%), and (V) Light and Hoechst image for no coating (b) adult human cardiomyocytes adhered per view as indicated, and scored using manual counting using ImageJ software, post  $1\times$  PBS wash after overnight incubation in the corresponding coatings. Data shown are the media  $\pm$  SD.  $n=4$  for all the conditions.

<http://dx.doi.org/10.1371/journal.pone.0069812.g003>

## Transfection of Human Adult Cardiomyocytes

Human adult cardiomyocytes were transfected using an oscillating magnet array on the magnefect-nanoII system at a frequency of 2 Hz with a 0.2 mm displacement. No difference in transfection efficiency between the cells coated with Collagen I ( $46.0\pm 4.0\%$ ) and ECM ( $44.8\pm 6.1\%$ ,  $p>0.05$ ) coated plates was observed. However, cells seeded onto uncoated plates exhibited low transfection efficiency ( $22.7\pm 4.2\%$ ,  $**p<0.01$ ) compared to the other conditions as shown in [Figure 4](#). The results demonstrate that oscillating magnetofection can transfect adherent cells efficiently when compared to semi-adherent cells. Following this we evaluated the oscillating nanomagnetic transfection technique against another adherent state transfection and a suspension state transfection methods i.e. lipid- and electroporation-based technologies.



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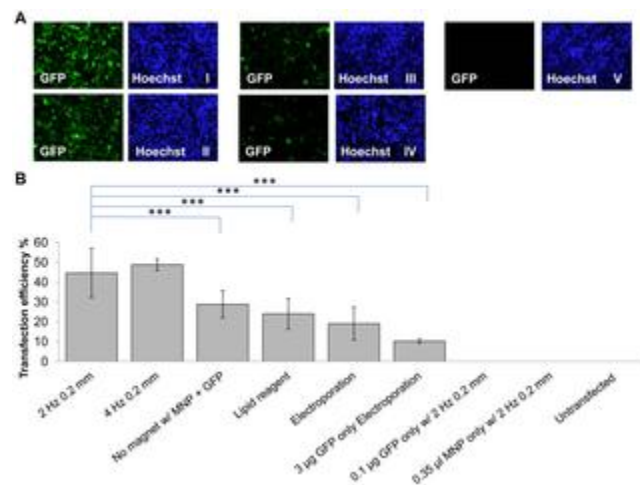
### Figure 4. Comparison of oscillating magnet array-based nanomagnetic transfection between adult human cardiomyocytes seeded onto rat tail collagen 1 coated and ECM coated plates.

(a) Fluorescent microscope images of adult human cardiomyocytes transfected with pEGFP-N1 representing each conditions, took 48 hrs post transfection. (I) GFP fluorescence and Hoechst image for 2 Hz 0.2 mm in collagen 1 coated (0.125  $\mu\text{g}/\mu\text{l}$ ) plate, (II) GFP fluorescence and

Hoechst image for 2 Hz 0.2 mm in ECM coated plate, and (III) GFP fluorescence and Hoechst image for 2 Hz 0.2 mm in un-coated plate (b) adult human cardiomyocytes were transfected with pEGFP-N1 as indicated, and scored using manual counting using Image J software, 48 h after transfection. Data shown are the media  $\pm$  SD. n=3 for all the conditions. (\*\*p<0.01- Statistically significant).

<http://dx.doi.org/10.1371/journal.pone.0069812.g004>

Cardiomyocytes transfected using the oscillating magnet array on the magnefect system at 4 Hz frequency/0.2 mm displacement (TE=48.8 $\pm$ 2.8%) and at 2 Hz 0.2 mm (TE=44.6 $\pm$ 12.4%) outperformed both a commonly used cationic lipid (TE=24.0 $\pm$ 7.8%, \*\*\*p<0.001) and electroporation (19.1 $\pm$ 8.3%, \*\*\*p<0.001). At 4 Hz 0.2 mm (48.8 $\pm$ 2.8%) and 2 Hz 0.2 mm (44.6 $\pm$ 12.4%) conditions cardiomyocytes showed significant increase in transfection efficiency when compared to no magnet control (28.8 $\pm$ 6.8%, p<0.001) as shown in [Figure 5](#). Overall these results demonstrate successful and efficient delivery of gene into cardiomyocytes using an oscillating magnet array and MNPs.



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**Figure 5. Comparison of oscillating magnet array-based nanomagnetic transfection over lipid based transfection and electroporation in adult human cardiomyocytes.**

(a) Fluorescent microscope images of adult human cardiomyocytes transfected with pEGFP-N1 representing each conditions, took 48 h post transfection. (I) GFP fluorescence and Hoechst image for oscillating magnet array-based nanomagnetic transfection performed at 2 Hz 0.2 mm, (II) GFP fluorescence and Hoechst image for oscillating magnet array-based nanomagnetic transfection performed at 4 Hz 0.2 mm (III) GFP fluorescence and Hoechst image for lipid based transfection reagent, (IV) GFP fluorescence and Hoechst image for electroporation and (V) GFP fluorescence and Hoechst image for untransfected (b) adult human cardiomyocytes were transfected with pEGFP-N1 as indicated, and scored using manual counting using Image J software, 48 h after transfection. Data shown are the media  $\pm$  SD. n=18 for oscillating magnet array-based nanomagnetic transfection at 2 Hz 0.2 mm. n=12 for lipid based transfection reagent. n=6 for oscillating magnet array-based nanomagnetic transfection at 4 Hz 0.2 mm,

electroporation and pEGFP-N1 only electroporation conditions. n=9 for no magnet. n=3 for pEGFP-N1 only, Neuromag only, and un-transfected conditions. (\*\*\*)p<0.001- Statistically significant).

<http://dx.doi.org/10.1371/journal.pone.0069812.g005>

## Cell Viability

Cell viability based on the CytoTox-ONE™ homogenous membrane integrity assay for human prenatal cardiac progenitor cells was: static magnetofection (90.8±10.4%); 2 Hz/0.2 mm (84.4±13.9%); and 4 Hz/0.2 mm (76.3±25.0%); n=3 for all groups. The cell viability based on cellTrace™ calcein red-orange AM staining for human adult cardiomyocytes was: no magnet (92.8±2.3%); 2 Hz/0.2 mm (89.7±5.6%); and 4 Hz/0.2 mm (69.5±8.4%); n=9 for all groups. Overall the results demonstrate that MNP-based gene delivery appears to have minimal impact on the viability of cardiac progenitor cells and cardiomyocytes at static and low frequencies, however, a decrease in viability with the increasing frequency was observed.

## Discussion

Recent studies have demonstrated that, in some cell types, the use of oscillating magnet arrays on the magnetofect system may enhance nanomagnetic gene transfection in comparison to static magnetofection [25], [26], [27]. It appears that cellular uptake of complexes during MNP mediated transfection is through endocytosis [28], especially through caveolae-mediated endocytosis in oscillating nanomagnetic gene transfection [16]. However, there may be effects due to oscillations that occur after the complex has been internalized that facilitate transfection.

Both cardiac progenitor cells and adult cardiomyocytes are important cell types for studies of the genetic basis of heart disorders such as atrioventricular conduction delay, atrial septal defects, early valve calcification and endocardial cushion effect. In order to understand these diseases and develop treatments, it is necessary to develop efficient and safe gene transfection techniques that also have the potential to be translated to the clinic. The oscillating nanomagnetic transfection technology demonstrated here outperforms other non-viral transfection techniques and, as MNPs are in clinical use as MRI contrast agents, has the potential to be translated into clinical application, such as transplantation of genetically altered cells.

In this study, we have shown that it is possible to optimize oscillating nanomagnetic transfection by investigating a range of frequencies and amplitudes. Similar transfection studies using oscillating nanomagnetic transfection on mouse embryonic fibroblasts, human umbilical vein endothelial cells [17], rat oligodendrocyte precursor cells [19], rat astrocytes [27], MG63 and NCI-H292 cells [29], [25] demonstrates the versatility of the frequency-displacement based-nanomagnetic transfection technology as well efficiency over a range of primary, differentiated, undifferentiated cells and cell lines. The reason behind frequency-displacement dependent transfection remains elusive; however, increased cytosolic Ca<sup>2+</sup> transients and enhanced Ca<sup>2+</sup> oscillations have been observed with increasing pacing frequency in adult mouse myocytes [30]. Similarly, shear stress induced cytosolic Ca<sup>2+</sup> transients are demonstrated in different cell types [31], [32]. The frequency-displacement dependent transfection we observe



may depend on the cytosolic  $\text{Ca}^{2+}$  oscillations, which is reported to interfere with the transfection and gene expression of cells [33], [34].

Moreover oscillating nanomagnetic transfection being an adherent cell transfection technique, we have also demonstrated that transfection efficiency can be enhanced by coating the wells with collagen. It is likely that increased efficiency in cells seeded onto rat tail collagen I was due to efficient adherence as collagen type-I is one of the fibrous proteins within extracellular matrix and, being a structural protein, it is highly biocompatible. In the cardiomyocytes, this led to increased adhesion and improved transfection efficiency with the oscillating system, while PEI and foetal bovine serum coating had a detrimental effect on the cells. This study represents a promising stepping stone towards a valuable research tool for cardiac gene therapy.

Oscillating nanomagnetic transfection optimisation may also be influenced by the properties of the MNPs used. While it is true that increases in the magnetic content (volume of magnetic material) of the particles will increase the magnetic force, generally the particles used for these studies are iron oxide/polymer composite particles. Increasing the hydrodynamic diameter is not always associated with a proportional increase in magnetic iron oxide as the polymer represents the bulk of the particle's volume. Previous studies on MNP-mediated gene delivery has shown that 100 nm MNPs (hydrodynamic diameter) were endocytosed through caveolae-mediated endocytosis [16]; 200 nm MNPs through clathrin- or caveolae-mediated endocytosis [35]; and 300 nm MNPs through macropinocytosis and clathrin-mediated endocytosis [36]. Receptor mediated endocytosis has been involved either totally or partially in these demonstrated entry mechanisms of different sized nanoparticles. A diameter of 50–60 nm is considered to be suitable for optimal receptor mediated endocytosis [37], however the hydrodynamic diameter of Neuromag used in this study ranges between 140–200 nm [27]. Clearly the magnetic force on the particles, while important, is only one parameter to be considered as different entry mechanisms may be associated with increased or decreased transfection efficiency. Still, MNP-mediated gene delivery depends to some degree on the attractive force exerted by the magnet array on the magnetic particles [25]. The attractive force is directly proportional to the volume of magnetic material in the particle, magnetic field strength/gradient of the magnet array and magnetic properties (susceptibility) of the particle [18]. Superparamagnetic nanoparticles have high magnetic susceptibility but are limited in size to diameters of roughly 30 nm or less for iron oxides (though this is somewhat dependent on aspect ratios as magnetite has strong shape anisotropy). Suitable biocompatible polymer coating/matrices are also important for enhancing transfection, alongside size and magnetic properties of the nanoparticles [28].

## Acknowledgments

We thank all our colleagues at nanoTherics Limited, and Institute for Science & Technology in Medicine, Guy Hilton Research Centre, Keele University for their support.

## Author Contributions



Conceived and designed the experiments: JL MS JD. Performed the experiments: MS. Analyzed the data: MS JL JD. Contributed reagents/materials/analysis tools: JL MS JD. Wrote the paper: MS. Edited the manuscript: JL JD.

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